



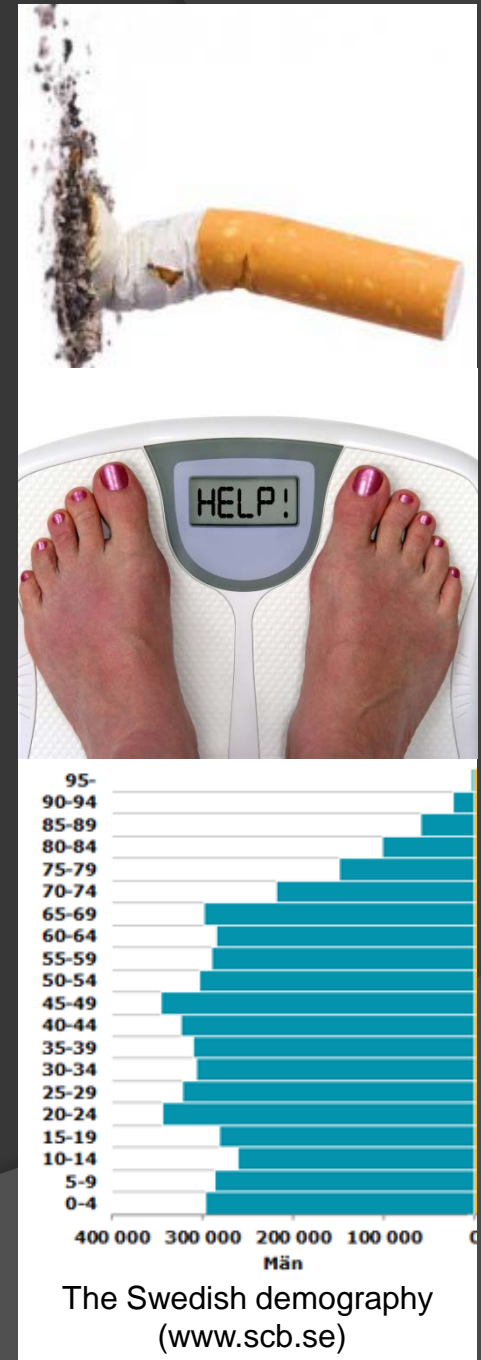
VR Project 2015 – 2018

IDENTIFICATION OF CONSTITUTIVE PARAMETERS IN ARTERIES

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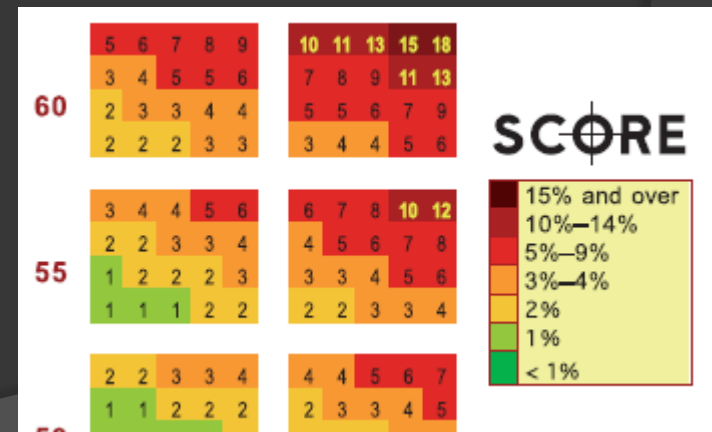
Motivation

- Cardiovascular (CV) diseases cause 40% of all deaths in the EU
- The total cost for CV diseases is 196 billion Euro
- Age, cholesterol, diabetes, hypertension, obesity, and smoking are risk markers



Motivation (cont'd.)

- Prediction of CV events, e.g., SCORE
- Underestimation of risk for single marker subjects
- Fluctuations in markers over time

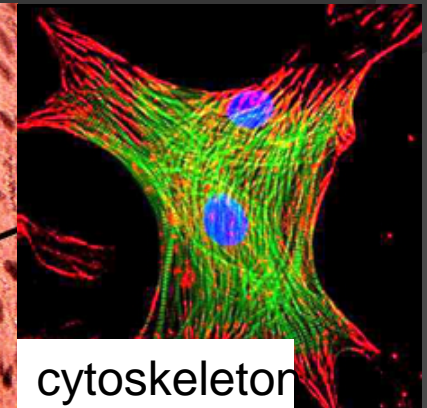
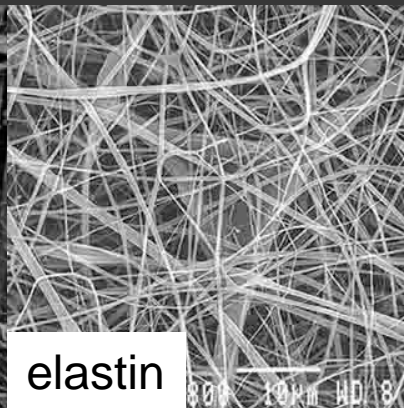
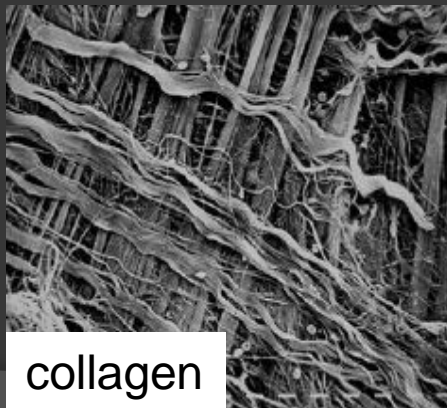
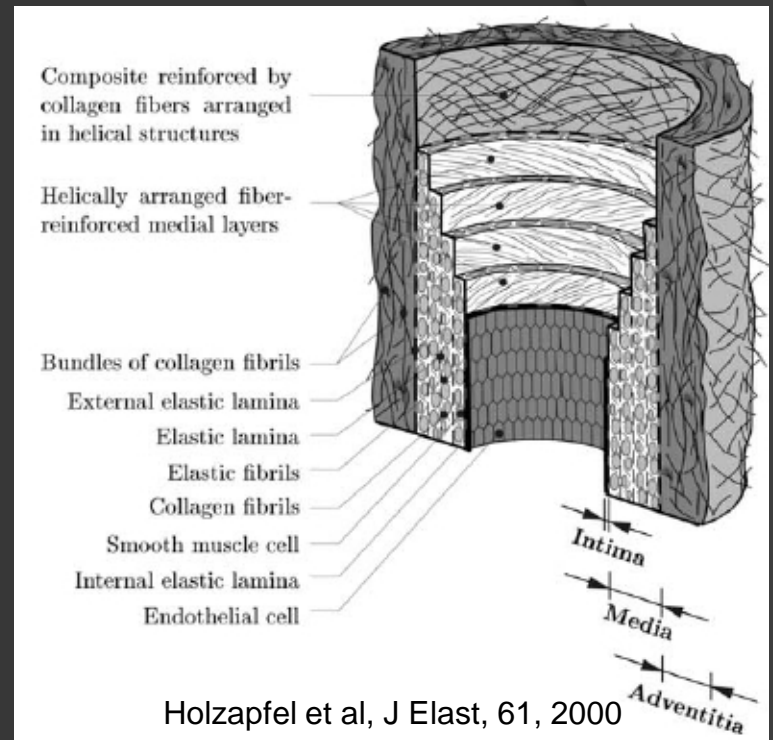


Motivation (cont'd.)

- ⦿ Arterial stiffness is a potential risk marker
- ⦿ Increased arterial stiffness is an essential ingredient to develop hypertension
- ⦿ Reflects the 'cumulative risk'

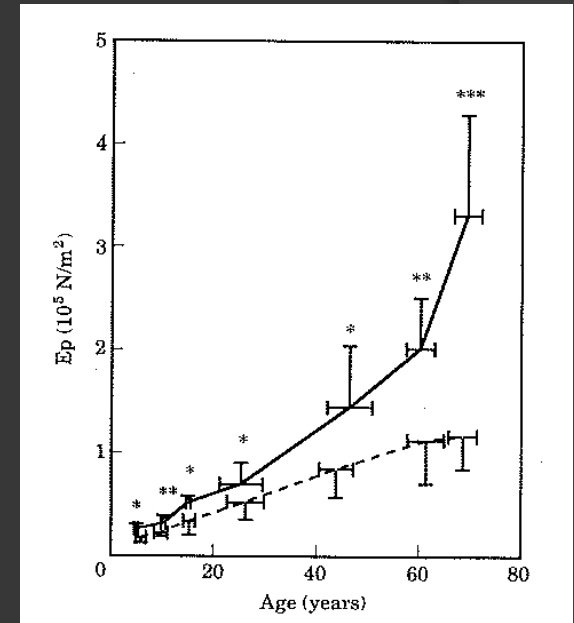
Physiology

- Extracellular matrix of collagen and elastin
- Circumferentially embedded smooth muscle (SM) cells
- Increases focal adhesion, intrinsic SM stiffness



Arterial Stiffness Estimation

- Clinical measures are crude
- Constitutive parameters from nonlinear models: van der Horst et al. (2012), Masson et al. (2008), Schulze-Bauer & Holzapfel (2003), Smoljkic et al. (in press), Stalhand and Klarbring (2005), Stalhand (2009), Astrand et al. (2011)
- Trade-off between details and identifiability and more complex



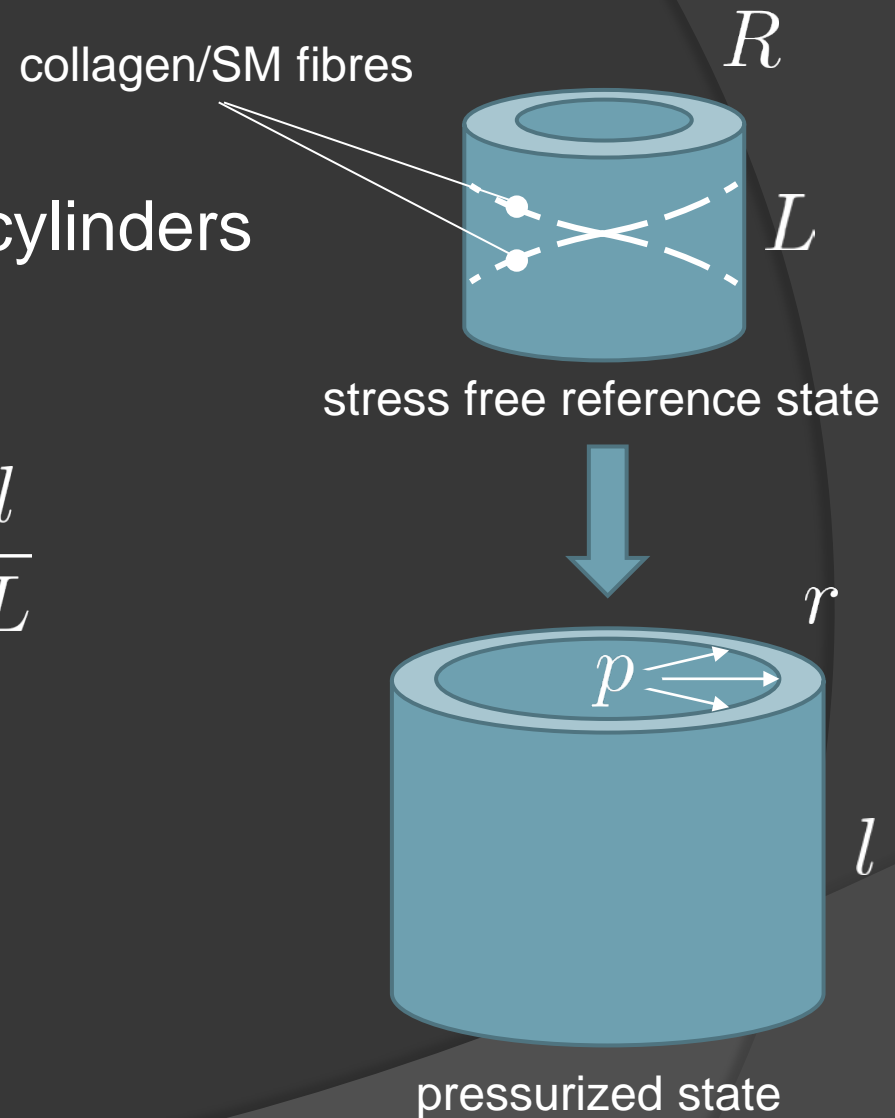
Kinematics

- Pressurized thin-walled cylinders
- Shear free inflation

$$\lambda_\theta = \frac{r}{R}, \quad \lambda_z = \frac{l}{L}$$

- Incompressibility

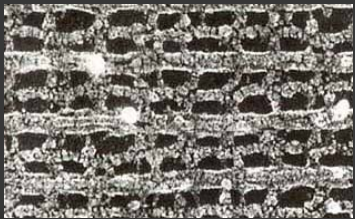
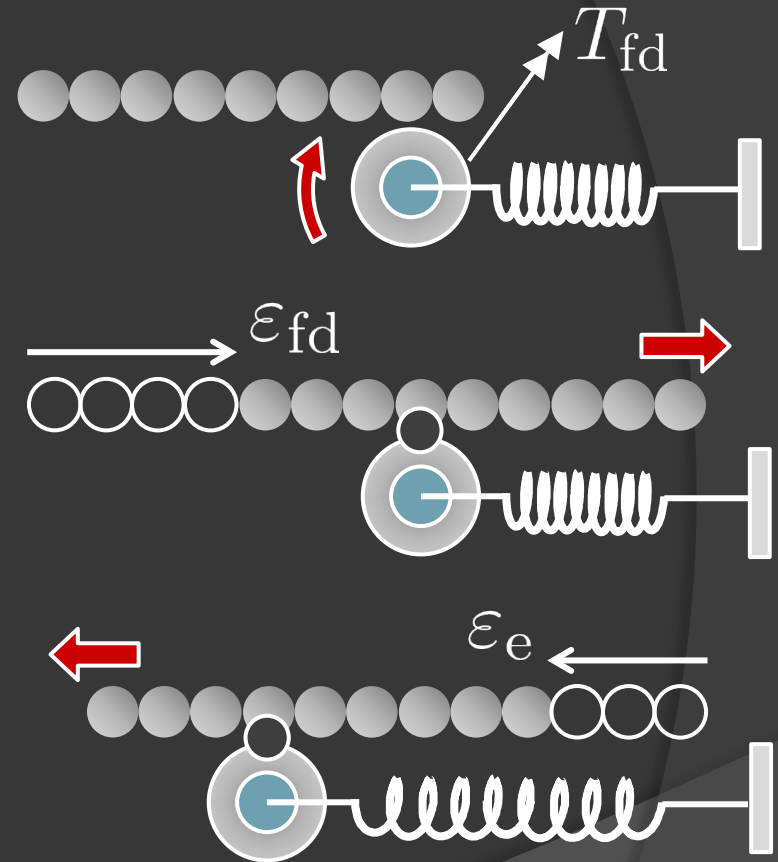
$$\lambda_\theta \lambda_z \lambda_r = 1$$



Kinematics (cont'd.)

- Active force generation by a spring-friction-clutch model
- Tangential smooth muscle arrangement

$$\lambda_\theta = \underbrace{\varepsilon_e}_{\text{elastic deformation}} + \underbrace{\varepsilon_{fd}}_{\text{filament translation}} + 1$$



Murtada et al, BMMB, 9, 2010



Constitutive Equations

- Dissipation inequality:

$$T_\theta \dot{\lambda}_\theta + T_z \dot{\lambda}_z + T_r \dot{\lambda}_r + T_{fd} \dot{\varepsilon}_{fd} - \dot{\psi} \geq 0$$

- Free energy:

$$\psi = \psi^p + \psi^a - p (\lambda_\theta \lambda_z \lambda_r - 1),$$

$$\psi^p = \psi^p(\lambda_\theta, \lambda_z, \lambda_r), \quad \psi^a = \psi^a(\varepsilon_e, \varepsilon_{fd})$$

Constitutive Equations (cont'd.)

$$T_\theta = -\frac{p}{\lambda_\theta} + \frac{\partial \psi^p}{\partial \lambda_\theta} + \frac{\partial \psi^a}{\partial \varepsilon_e} \quad (\text{first P-K stress})$$

$$T_z = -\frac{p}{\lambda_z} + \frac{\partial \psi^p}{\partial \lambda_z}$$

$$T_r = -\frac{p}{\lambda_r} + \frac{\partial \psi^p}{\partial \lambda_r}$$

$$T_{fd} - \frac{\partial \psi^a}{\partial \varepsilon_{fd}} + \frac{\partial \psi^a}{\partial \varepsilon_e} = c \dot{\varepsilon}_{fd} \quad (\text{evolution law})$$

$$\sigma_k = \lambda_k T_k, \quad (\text{Cauchy stress})$$

Free-energy functions

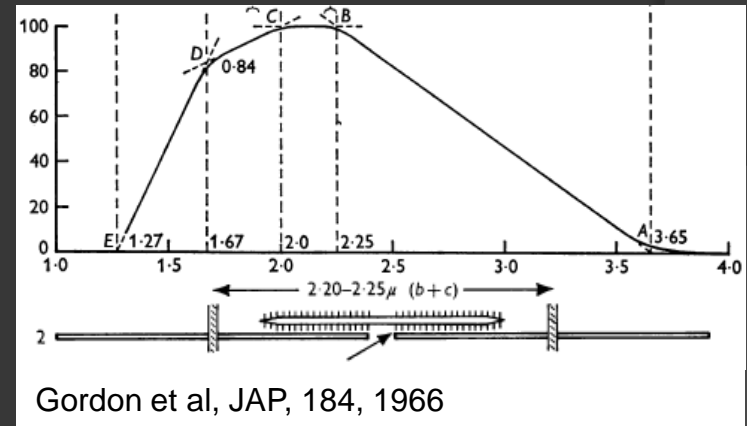
- Passive tissue (tangential collagen):

$$\psi^p = \frac{c_0}{2} (\lambda_\theta^2 + \lambda_z^2 + \lambda_r^2 - 3) + \frac{c_1}{c_2} (\exp\{c_2(\lambda_\theta^2 - 1)^2\} - 1)$$

- Actomyosin network (linear strain energy):

$$\psi^a = \frac{1}{2} f K_e \varepsilon_e^2$$

$$f = \exp\left\{ \left(\varepsilon_a^0 - \varepsilon_a \right)^2 / 2\gamma^2 \right\}$$



Specialized Evolution Law

- ⦿ Quasi-static conditions: $\dot{\varepsilon}_{fd} = 0$
- ⦿ Non-cycling (latch) cross-bridges: $T_{fd} = 0$
- ⦿ Specialized evolution law:

$$f \varepsilon_e - \frac{1}{2} \frac{\partial f}{\partial \varepsilon_{fd}} \varepsilon_e^2 = 0$$

Parameter Estimation

- ⊙ Wire myograph
 - 1D
- ⊙ Pressure-radius response
 - Incomplete data
 - Reference geometry?
 - Multiple minima

Passive			Active			Geom	
c_0	c_1	c_2	K_e	ϵ_{fd}^0	γ	L	R

